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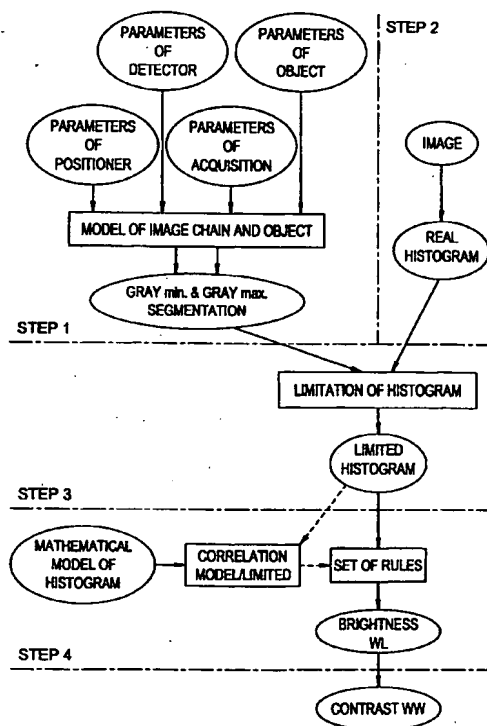
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(54) **Method of automatic determination of the contrast and brightness of a digital radiographic image**

(57) The method comprises a histogram of the radiographed image, i.e., a real histogram (step 2), a mathematical model of the image chain and the object obtained by calibration. The mathematical model of the image chain and the object and a set of parameters of acquisition, of the detector, of the positioner and of the object are used to determine (step 1) two values of gray level, gray min and gray max, delimiting a useful zone and the part below gray min and the part above gray max are suppressed (step 3) in the real histogram, i.e., a limited histogram. A set of rules is applied (step 4) to the limited histogram in order to determine the level of brightness (WL) and the contrast (WW) is obtained from the brightness and possibly from one or more parameters selected by the user or fixed a priori.

**FIG. 1**



## Description

[0001] This invention relates to a method for automatic determination of the brightness and contrast of a digitized radiographic image of an object.

[0002] It finds a particularly interesting application in the medical field in which fine analyses of radiographic images are made, notably mammography.

[0003] In the medical field, diagnoses generally are based on the study of a radiographic image. The progress of digital systems now makes it possible to vary the characteristics of the image in order to best effect a diagnosis. Thus, it is evident that the quality of the image is an essential point.

[0004] As is well known, image acquisition introduces numerous parameters related to the acquisition chain: These include the parameters of acquisition (target material of the anode of the X-ray tube [track], material and thickness of the filter at the output of the X-ray tube [filter], voltage applied between cathode and anode of the X-ray tube [kV], heating current of the filament of the cathode of the X-ray tube [mA], exposure time, ...), the parameters of the positioner (incidence of the view, enlargement factor, type of compression pad used, thickness of the object, force of compression, ...) and the parameters of the digital detector (relation of gray levels to flux of X-rays captured ...). In addition to this, the parameters of the object, in particular its composition, are introduced. This set of parameters makes it possible to obtain an image that is in fact composed of pixels of shades of gray. Quantification of the image is obtained on a given number of gray levels. When the image is displayed on a screen or imprinted on a film using a given range of gray levels, the contrast perceived may be considerably different among images of the same object acquired with different sets of parameters of acquisition or among images of different objects obtained with the same set of parameters. In addition, selection of the range of gray level to be considered for the screen is of great importance in order to give an acceptable perception of contrast in the image. Thus, once the image has been obtained, the user interactively modifies the brightness (WL: window level) and the contrast (WW: window width) of this image in order to adjust the range of gray levels in it so as to obtain a correct perception of contrast.

[0005] Generally, for more than 16000 different gray levels, it is a difficult and lengthy task to select the correct brightness and contrast manually.

[0006] An embodiment of the invention permits automatically determining the value of the brightness (WL) and to derive the contrast (WW) from it.

[0007] An embodiment of the invention therefore proposes a method of digital radiographic image acquisition of an object with automatic adjustment of the parameters of visualization (brightness, contrast). The method is adaptable, since the wishes of the user may be taken into account.

[0008] This method comprises the obtaining of two gray levels, min gray and max gray, revealing a zone of gray levels in which the brightness (WL) is capable of being determined, a set of rules for calculation of the value WL, and from this, lastly, the derivation of a range of gray levels for the contrast WW.

[0009] Other advantages and characteristics of the invention will appear upon examination of the detailed description of a mode of implementation, in no way limitative, and of the accompanying drawings, wherein:

Figure 1 is a flow chart of a mode of implementation of the method according to an embodiment of the invention;

Figure 2 illustrates the limited histogram with respect to the real histogram;

Figure 3 illustrates a way of selecting WL;

Figure 4 describes the method of obtaining an invariant contrast.

[0010] According to a general embodiment of the invention, a first step, segmentation, is carried out. The input data of this first step are the parameters of acquisition, the parameters of the digital detector, the parameters of positioning and the parameters of the object. All of these parameters are input in a pre-established mathematical model of the image chain and of the object.

[0011] The model makes it possible to determine a gray min level and a gray max level. The part surrounded by these two levels is the useful zone of gray levels within which the value of the level of brightness WL will be selected.

[0012] This step corresponds to segmentation of the image by double thresholding so that only the points of the image having gray min level and gray max level are preserved.

[0013] A second step is carried out in parallel with the preceding step. It performs the real radiographic acquisition of the object. From the image obtained, a histogram is drawn up, i.e., a real histogram.

[0014] The third step introduces gray min, gray max and the real histogram. Their correlation results in suppression in the real histogram of the part below the level of min gray and of the part above the level of max gray. The result of the third step is an interval of gray levels limiting the useful zone, i.e., limited histogram. The value of the brightness WL within this interval then remains to be determined.

[0015] Accordingly, the fourth step concerns the determination of WL, which may be done by means of a set of simple rules known to persons skilled in the art. This set of rules makes it possible to obtain a value WL. However, when the user performs numerous mammographies, it is necessary to improve efficiency by introducing a mathematical model of the histogram. One

model is described by Mr. Jean Lierrard, LSD/AAP reference 98030 Technical Note GE Medical Systems, August 1998. It considers a compressed breast, the shape of which is modeled, for example, with the aid of simple geometric forms. When data of the breast to be mam-

mographed are introduced, a histogram model characterized by a maximum at the level of radiologic thickness corresponding to a breast tissue is obtained.

[0016] Correlation of the mathematical model of the histogram so determined and the limited histogram makes it possible to determine the value of a radiologic thickness characterizing the breast.

[0017] The limited histogram, thus refined, will be subject to a set of rules permitting determination of the brightness WL.

[0018] The fifth step concerns determination of the contrast WW. This value may be obtained in a manner known to those skilled in the art by introducing the value WL and any parameters known a priori and dependent upon the user.

[0019] According to one mode of implementation of the invention, the contrast WW may alternatively be determined independently of WL. In this case, the coefficient of mean attenuation ( $\mu$  mean), dependent upon the spectrum, is used. In a general way, the WW thus obtained is a function of the spectrum, because it is proportional to  $\mu$  mean.

[0020] Obtaining WL and WW (independently of WL) is equivalent in fact to an auto-contrast operation that may be used in a method of perception of contrasts in invariant thickness.

[0021] An embodiment of this method makes the perception of contrasts independent of the conditions of acquisition and of the object. For two objects of different thicknesses, it is desired that regardless of the conditions of acquisition, the contrast perceived on the image should remain faithful to their difference in real thicknesses.

[0022] In other words, it is desired that a given thickness should always represent the same perception of contrast, regardless of what the object and the conditions of acquisition are.

[0023] In effect, in the course of image acquisition, the physical elements cause the spectrum to convert the real thickness of the object into radiologic thickness, thus resulting in a perception of unfaithful contrast. This is an effect of exponential attenuation. The effect is compensated for by introducing into an image chain a change-of-space step in order to annul the exponential attenuation due to interaction of the X-rays with the object by employing a modified logarithmic function. The change of space makes it possible to leave the exponential space to pass into the space of radiologic thicknesses.

[0024] Likewise introduced is a visualization step making it possible to pass from the space of radiologic thicknesses to the space of real thicknesses. This change of space is possible because WW is proportional to the coefficient of mean linear attenuation of the ob-

ject studied and independent of WL.

[0025] Although the invention is not limited, the method is applicable to the automatic determination of the brightness WL and of the contrast WW for a mammography.

[0026] As shown in Figure 1, the first step employs a mathematical model of the image chain and the object with, in input data, the following parameters:

- thickness of the compressed breast and parameters of the positioner (incidence of the view, enlargement factor, type of compression pad used, thickness of the object, force of compression, ...) as parameters of the positioner,
- parameters of the detector (relation between the flux of X-rays received on the detector and the gray levels of the image produced, ...)
- parameters of acquisition (track, filter, kV, mAs, ...)
- parameters of the object (mechanical thickness of the breast, minimum  $\mu$  min and maximum  $\mu$  max values of the coefficient of linear attenuation of the object, ...).

[0027] Since the breast is composed principally of fibrous and adipose tissues, if there is no information on the composition of the breast,  $\mu$  min and  $\mu$  max may be estimated by making two extreme assumptions.

[0028]  $\mu$  min corresponds to the coefficient of linear attenuation of the least attenuant tissues of the object (adipose tissues for the breast) for the energies of the X-ray spectrum determined by the parameters of acquisition.

[0029]  $\mu$  max may be estimated in two ways: on the one hand like  $\mu$  min; by considering that  $\mu$  max corresponds to the coefficient of linear attenuation of the most absorbent tissues of the object (fibers for the breast) for the energies of the X-ray spectrum determined by the parameters of acquisition; on the other hand, in a more precise manner, from a mathematical model of the image chain, the mechanical thickness of the compressed breast, the parameters of acquisition and a quantity of photons obtained following preexposure performed on a zone of maximum density (which makes it possible to estimate the value of the coefficient of linear attenuation corresponding to the most attenuant zone of the object).

[0030] The set of parameters introduced into the mathematical model of the image chain and the object makes it possible to have two values of gray levels, gray min and gray max, at the output (Fig. 2). These two values, as a matter of fact, delimit the useful zone, which is a zone of gray levels relating really to the breast. In effect, owing to the two extreme values of the composition of the breast,  $\mu$  min and  $\mu$  max, a zone delimited by two extreme values, gray min and gray max, has been obtained, outside of which the gray levels do not corre-

spond to the breast. More precisely, the part of gray levels below gray min corresponds to objects more attenuant than the object of interest, and the part of gray levels above gray max corresponds to the bottom of the image. This step is a segmentation step because it makes it possible to delimit the useful zone.

[0031] Then a correlation is effected between the two values gray min and gray max and a histogram obtained from the radiographic image of the breast, i.e., a real histogram. More precisely, the part below gray min and the part above gray max are eliminated so as to preserve only the useful zone: limited histogram (Fig. 2).

[0032] The brightness WL is a value included in the useful zone and may be obtained in a variety of ways.

[0033] One manner of obtaining WL is the application of a set of pre-established rules to the limited histogram. A set of rules may include:

- determination of the gray level corresponding to the maximum of the limited histogram
- preservation of a quantity of x% (typically 95%) of occurrences of the limited histogram on the right of the maximum, and likewise x% of occurrences on the left of the maximum: a reconstructed histogram is thus obtained
- determination of WL as median value of the reconstructed histogram (Fig. 3).

[0034] It is alternatively possible to obtain WL with better precision by preceding the set-of-rules step by a correlation step. This step introduces a mathematical model of the histogram in which:

- the shape of the breast is a cylinder generated by rotation about an axis of a rectangle of which one of the short sides is closed by a semicircle equal in diameter to the length of this short side
- the composition of the breast is homogeneous, for example 100% fat
- a histogram is established that corresponds to probability as a function of the radiologic thickness of the breast
- the maximum of the histogram obtained represents the maximum thickness of the breast which, multiplied by the coefficient of attenuation, gives the maximum radiologic thickness corresponding to the adipose tissue (fat).

[0035] Correlation of the two histograms (mathematical model and limited histogram) makes it possible to determine in the limited histogram the value of the maximum radiologic thickness corresponding to the adipose tissue in the breast.

[0036] This then makes it possible to determine the values of radiologic thickness of the various components of the breast.

[0037] This correlation is performed by employing a method of minimization of errors between two functions such as, for example, the method of least squares.

[0038] An appropriate set of rules can then be applied in order to determine WL. For example,  $WL = \alpha E$ , with E representing the value of the radiologic thickness obtained from the mathematical model of the histogram.

[0039] The following step corresponds to the determination of WW by using WL. Thus, WW is obtained from a function introducing WL

and possibly other parameters, in particular a parameter G (Fig. 3), which is selected by the user.

[0040] This parameter G therefore makes the method adaptable to each user.

$$WW = g(WL, G)$$

g being a function which, from WL and G, determines WW, which thus represents a range of gray levels about WL.

[0041] It is alternatively possible to determine WW independently of WL.

[0042] First,  $\mu$  mean is determined from information drawn from the limited histogram. As an example, the  $\mu$  corresponding to the median value of the limited histogram may be taken as  $\mu$  mean.

[0043] Then, a law introducing a constant Cte is used in order to derive WW from it:

$$WW = Cte \mu (\text{spectrum})$$

[0044] This relation is true in a mono-energetic case, but in a general way, WW is a function of the spectrum

$$WW = f (\text{spectrum})$$

[0045] The operation of auto-contrast has thus been performed, since WL and WW have been established.

[0046] The way in which perception of the contrast of a difference in thickness remains invariant regardless of the means of acquisition and the objects will now be explained with reference to Figure 4.

[0047] The imposition of X-rays on the object results in an exponential attenuation of the intensity I at the level of the image:

$$I = I_0 \exp (-\int \mu dl)$$

[0048]  $I_0$  is a constant, 1 represents an infinitesimal magnitude that corresponds to a distance along the path connecting the focus of the X-ray and the detector.

[0049]  $\int \mu dl$  represents the radiologic thickness for a given zone of an object.

[0050] It is this quantity that interests us. To obtain it, a pre-LUT (look-up table) operation is performed, making it possible to offset the exponential attenuation by using a modified logarithmic function. It is called modified because the lowest gray levels are converted according to a linear rotation when the logarithmic function is progressively introduced for the other gray levels.

[0051] We thus find ourselves in the space of radiologic thicknesses in which a radiologic thickness may be given the notation  $\mu H$ , with  $H$  the real thickness.

[0052] Lastly, a change of space must be made to get back into the space of real thicknesses.

[0053] Auto-contrast furnishes us with the values  $WW$  and  $WL$ , which are introduced at the level of a visualization lut. The said visualization lut makes it possible to eliminate  $\mu$ . In the case of a mono-energetic image, this operation amounts to division by  $\mu$ .

[0054] This operation is possible because  $WW$  is proportional to  $\mu$ .

[0055] The result thus obtained may be introduced into the DICOM standard visualization system (Grayscale Standard Display Function, Supplement 28), familiar to persons skilled in the art, in order to visualize the image (Fig. 4).

#### Claims

1. A method of acquisition of a digital radiographic image of an object, having a histogram of the radiographed image (real histogram) and a mathematical model of the image chain and the object obtained by calibration, comprising the steps of:
  - a) providing the mathematical model of the image chain and the object and of a set of parameters of acquisition, of the detector, of the positioner and of the object, to determine two values of gray level, gray min and gray max, delimiting a useful zone
  - b) suppressing the part below gray min and the part above gray max in the histogram (limited histogram);
  - c) applying a set of rules to the limited histogram in order to determine the level of brightness  $WL$ ; and
  - d) obtaining the contrast  $WW$  from  $WL$  and possibly from one or more parameters selected by the user or fixed a priori.
2. The method according to claim 1, comprising the step of estimating a coefficient of minimum linear attenuation ( $\mu_{\min}$ ) of the object from known values of the coefficient of linear attenuation of the least attenuant tissues of the object (adipose tissues for the breast) for the energies of the X-ray spectrum determined by the parameters of acquisition and makes it possible, with the parameters of the detector, the parameters of the positioner, the parameters of acquisition and the parameters of the object, through a mathematical model of the image chain and of the object, to determine gray min.
3. The method according to claim 1, comprising the step of estimating a coefficient of maximum linear attenuation ( $\mu_{\max}$ ) of the object either from known values of the coefficient of linear attenuation of the most attenuant tissues of the object (fibrous tissue for the breast) for the energies of the X-ray spectrum determined by the parameters of acquisition or, in a more precise manner, from the mechanical thickness of the compressed breast, the parameters of acquisition, the mathematical model of the image chain and the object and from a quantity of photons obtained following a preexposure performed on a zone of maximum density of the object, and makes it possible, with the parameters of the detector, the parameters of the positioner, the parameters of acquisition and the parameters of the object, to determine gray min through a mathematical model of the image chain and the object.
4. The method according to any one of the preceding claims, wherein the limitation of the histogram introduces two gray levels (gray min and gray max) surrounding a zone of gray levels within which the brightness  $WL$  is determined.
5. The method according to any one of the preceding claims, wherein a correlation is made between the limited histogram and a mathematical model of the histogram in order to determine the value of a radiologic thickness characterizing the object.
6. The method according to claim 5, wherein the correlation between the limited histogram and the mathematical model of the histogram is effected by applying a method of minimization of errors between two functions.
7. A method of acquisition of a digital radiographic image of an object, having an acquisition chain comprises a step of compensation for the effect of exponential attenuation of the radiation by using a modified logarithmic function, so that perception of the contrast ( $WW$ ) of a given difference of thickness remains invariant regardless of the means of acquisition.
8. The method according to claim 7, wherein the brightness ( $WL$ ) and ( $WW$ ) obtained from a coefficient

cient of mean attenuation of the image independently of the brightness, are introduced in a visualization step so that the signals coming from the compensation step (space of radiologic thicknesses) are sized in the space of real thicknesses.

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FIG. 1

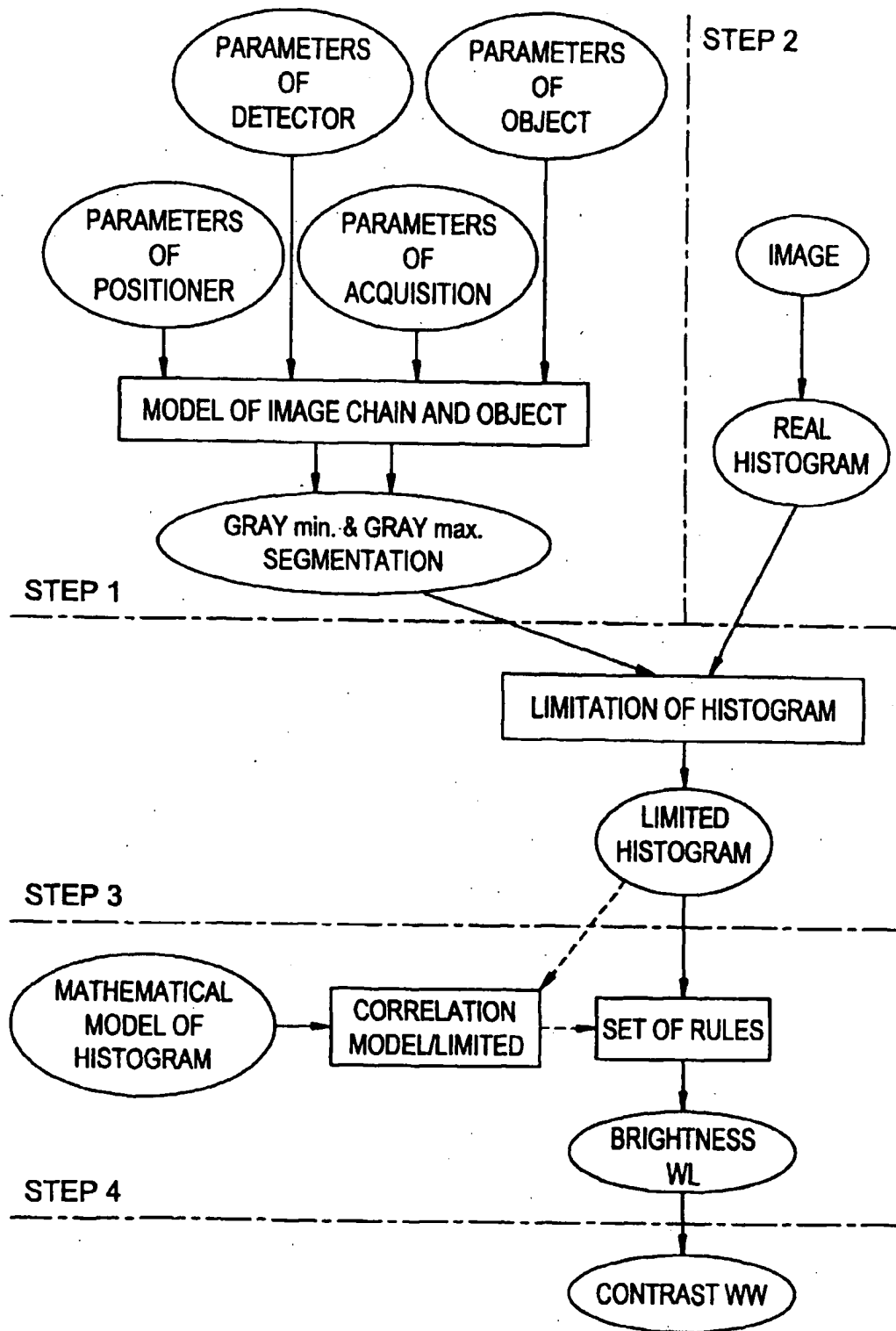


FIG. 2

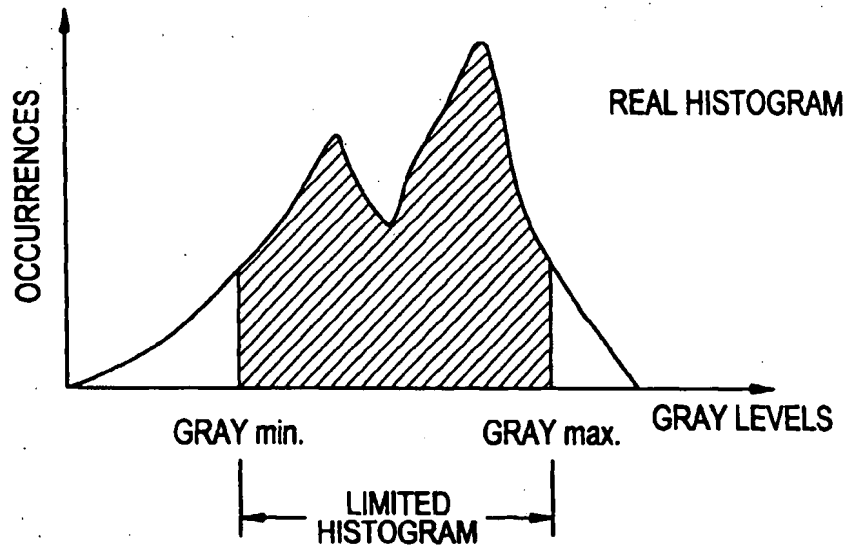


FIG. 3

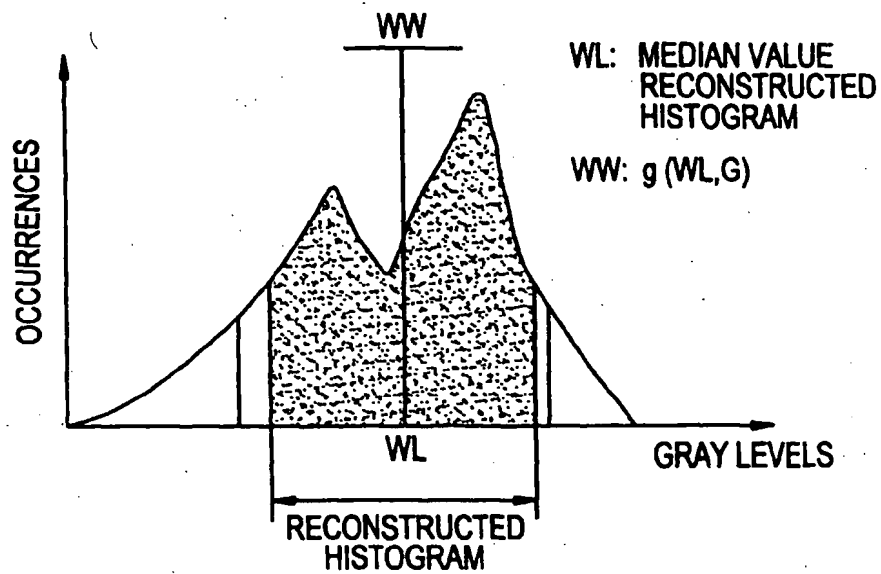
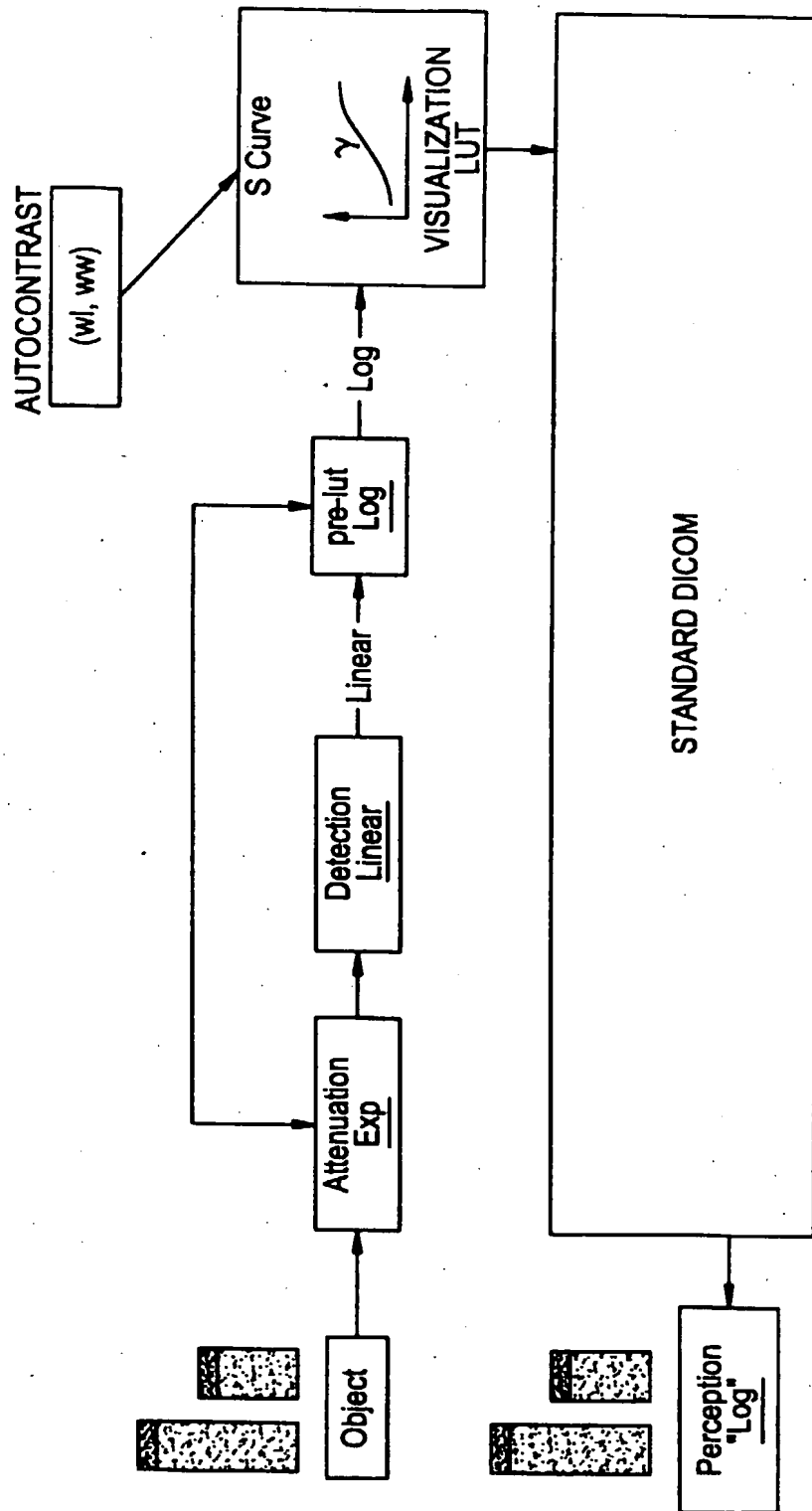




FIG. 4





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# EUROPEAN SEARCH REPORT

Application Number  
EP 99 30 9468

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.7)
X	US 5 696 805 A (PAWLICKI THADDEUS FRANCIS ET AL) 9 December 1997 (1997-12-09) * abstract; figures 8,9 *	1	G06T5/00
X	DE 32 14 725 A (PHILIPS PATENTVERWALTUNG) 27 October 1983 (1983-10-27) * abstract * * claims 1,2 *	1	
A	WO 98 37738 A (DIRECT RADIOGRAPHY CORP.; SCHWENKER EMILY J & LF (US); WILLIAMS C.) 27 August 1998 (1998-08-27) * page 3, line 14 - page 5, line 5; figures 3,4 *	1	
A	US 4 887 305 A (SHIMURA KAZUO) 12 December 1989 (1989-12-12) * abstract; figure 1 *	1	
A	EP 0 374 328 A (SHIMADZU CORP) 27 June 1990 (1990-06-27) * abstract; figure 1 *	7,8	TECHNICAL FIELDS SEARCHED (Int.Cl.7)
A	US 5 544 219 A (MULLER SERGE ET AL) 6 August 1996 (1996-08-06) * abstract * * column 4, line 1-12; figure 3A *	1,7	G06T G06F A61B G01T
The present search report has been drawn up for all claims			
Place of search BERLIN		Date of completion of the search 7 February 2000	Examiner Jonsson, P.O.
<p>CATEGORY OF CITED DOCUMENTS</p> <p>X: particularly relevant if taken alone Y: particularly relevant if combined with another document of the same category A: technological background O: non-written disclosure P: intermediate document</p> <p>T: theory or principle underlying the invention E: earlier patent document, but published on, or after the filing date D: document cited in the application L: document cited for other reasons &amp;: member of the same patent family, corresponding document</p>			

EPO FORM 1503 03.92 (PC/031)



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Application Number  
EP 99 30 9468

**CLAIMS INCURRING FEES**

The present European patent application comprised at the time of filing more than ten claims.

- ☐ Only part of the claims have been paid within the prescribed time limit. The present European search report has been drawn up for the first ten claims and for those claims for which claims fees have been paid, namely claim(s):
- ☐ No claims fees have been paid within the prescribed time limit. The present European search report has been drawn up for the first ten claims.

**LACK OF UNITY OF INVENTION**

The Search Division considers that the present European patent application does not comply with the requirements of unity of invention and relates to several inventions or groups of inventions, namely:

see sheet B

- ☐ All further search fees have been paid within the fixed time limit. The present European search report has been drawn up for all claims.
- ☒ As all searchable claims could be searched without effort justifying an additional fee, the Search Division did not invite payment of any additional fee.
- ☐ Only part of the further search fees have been paid within the fixed time limit. The present European search report has been drawn up for those parts of the European patent application which relate to the inventions in respect of which search fees have been paid, namely claims:
- ☐ None of the further search fees have been paid within the fixed time limit. The present European search report has been drawn up for those parts of the European patent application which relate to the invention first mentioned in the claims, namely claims:



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Office

**LACK OF UNITY OF INVENTION**  
**SHEET B**

Application Number  
EP 99 30 9468

The Search Division considers that the present European patent application does not comply with the requirements of unity of invention and relates to several inventions or groups of inventions, namely:

**1. Claims: 1-6**

A method of acquisition of a digital radiographic image of an object for determining automatically the brightness and contrast by means of a histogram

**2. Claims: 7,8**

Method of acquisition of a digital radiographic image comprising steps for compensating the exponential attenuation of the radiation by using a logarithmic function

**ANNEX TO THE EUROPEAN SEARCH REPORT  
ON EUROPEAN PATENT APPLICATION NO.**

EP 99 30 9468

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.  
The members are as contained in the European Patent Office EDP file on  
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07-02-2000

Patent document cited in search report		Publication date	Patent family member(s)		Publication date
US 5696805	A	09-12-1997	NONE		
DE 3214725	A	27-10-1983	NONE		
WO 9837738	A	27-08-1998	AU	6660098 A	09-09-1998
US 4887305	A	12-12-1989	JP	1947307 C	10-07-1995
			JP	6071300 B	07-09-1994
			JP	63233658 A	29-09-1988
EP 0374328	A	27-06-1990	DE	3888687 D	28-04-1994
			DE	3888687 T	06-10-1994
US 5544219	A	06-08-1996	FR	2712415 A	19-05-1995

EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82